

Treatment Techniques in External Beam Radiation Therapy: A Review

Sant Pal Singh^{1*}, Asita Kulshreshtha^{1*}, Anoop Kumar Srivastava² & Sumit Kumar Srivastava¹

¹Amity School of Applied Sciences, Amity University Uttar Pradesh, Lucknow
²Dept. of Radiation Oncology, Dr. RML Institute of Medical Sciences, Lucknow

DOI: 10.29322/IJSRP.11.09.2021.p11706
<http://dx.doi.org/10.29322/IJSRP.11.09.2021.p11706>

Abstract- Radiation therapy being most general treatment modality to cure patients with different malignancies covers more than fifty percent of cancer burden. Since its inception for treatment of cancer and other malignancies in 1896, development of new devices from time to time has brought several changes in techniques of radiation therapy. The present study aims to present an outlook towards the basic concepts involved related to radiation therapy and to highlight the development of the various techniques of radiation therapy involving wide range of energies from x-ray, γ -ray and charged particles. This presentation gives an outlook for various advanced techniques of radiation therapy like external beam radiation therapy, intensity modulated radiation therapy, image guided radiation therapy, stereotactic radiation therapy, brachy-therapy etc. This study gives an introduction of utilization of x-rays, γ -rays, photon beams and light charged particles i.e. electrons as a source of radiation used for radiation therapy and it is concluded that the electron beam therapy is more suitable for superficial tumors like nasal nodes, head and neck cancers and breast carcinomas. It is also beneficial in providing the radiation boost to the residual cancers after surgery. Since the energy of the beam drop off rapidly after the desired depth, so that the sensitive body parts can be escaped from the radiation effects.

Index Terms- Electromagnetic radiation, brachytherapy, computed tomography, radiation boost, biomedical imaging, on board imaging and multileaf collimators etc.

I. INTRODUCTION

Utilization of ionizing radiations were initiated to treatment of cancer and other malignancies just after the introduction of x-rays (a pattern of electromagnetic radiation) by German Professor Wilhelm Conrad Röntgen in 1895 and detection of radium by Marie Curie 1898 [1,2]. Radiobiological properties of x-rays and radium were recognized just after their evolution. Within a year of diagnosis of x-rays, Emil Herman Grubbe of Chicago assembled his first x-ray machine and used it for treatment of breast carcinoma in 1896 [3]. First conference concerned with contribution of radiation physics in medicine was organized in 1913. In early days of radiation therapy, x-rays and radium were only source of radiation for therapeutic cure of cancer as well as other malignancies and achieving around 20% of curable treatment [4]. Radiation physicists dealing with x-rays and gamma rays faced skin burns and many matured non-healing ulcers that predict towards biological properties of these radiations [5].

Diagnostic and therapeutic utilizations of radiation led to revolutionary changes in the field of medical science. Depending on radiobiological properties of radiations they are used in treatment of cancers, non-healing ulcers and other skin diseases [6-8]. H. Strebel from Germany in 1903 and R. Abbe from New York in 1904 respectively were the first, who used these radiations in interstitial brachytherapy [9,10]. Cancers of cervix was successfully treated with brachy-therapy in 1913 at congress organized at Halle. Brachytherapy was only technique for treatment of most of the patients suffering with cancer of cervix [11]. Three Physicists, for their discoveries related to radiations received Nobel Prize in late nineteenth century as golden era of Physics. Several other developments in this field took place such as production of isotopes, radiobiology and the three dimensional (3D) dosimetry [12-18]. Successive development of computed tomography (CT), magnetic resonance imaging (MRI), positron emission tomography (PET) and other advanced imaging techniques led to dosage prescription and treatment plan from print to volume and also single plane dosimetry to multiple plane dosimetry [19]. Discoveries of basic radiation sciences (i.e. x-rays and γ -rays) direct towards keen understanding of human body disorders and treatments techniques lead to revolutionary development in medical sciences and diseases managements [20-23].

II. METHODS AND MATERIALS

2.1 Computed Tomography and its Development

A revolutionary improvement took place in radio-diagnosis as well as radiation therapy planning of cancer with the development of advanced imaging techniques like CT (figure 1), MRI and PET-CT. Initially, it was very difficult to determine radiation dose distribution in different sites and organs of human body for irradiation. Isodose charts obtained from homogeneous medium (water equivalent) were the only basis of radiation dose calculations [24,25]. However, there are many distortions due to inhomogeneities of human body and hence estimation of exact dose of radiation inside body was not possible. The exact absorption pattern, electron fluence and point to point dose corrections were needed to plan accurate radiation therapy. It was not possible with the conventional treatment techniques so that for deep rooted tumors one has to guess relative position of tumor and normal tissues.

Utility of x-rays were redeemed with emergence of CT in 1971 by Dr. G.N. Hounsfield and EMI Ltd. They developed the first commercial system capable of image reconstruction from x-

rays projections in 1972 [26]. These systems were trialed with γ -rays source in experimental mode and later on replaced by x-rays-source. Ledly in 1974 developed the first whole body scanner with ameliorated spatial resolution which was used for CT supported treatment planning [27].

Later on advanced mathematical principles were used in image reconstruction algorithms to have higher resolutions. These CT scanners can scan pictures in few seconds or less with higher resolution and sensitivity. Advance CT treatment plannings improve outcomes of radiation therapy such as various inhomogeneities inside body like air cavities (lungs, oral cavity, nasal cavity etc.), bones and tissues of different densities and composition. More quantitative and precise information regarding patient cross-section, shape and composition (effective atomic number, density etc.) of inhomogeneities are available with advanced CT scanners [28]. Various stages of the developments in computed tomography is given below-

2.2.1 First generation: First generation of computed tomography is based on the concept of rotate/translate system of pencil beam of x-rays. Pencil beam of x-rays was produced by using a pinhole collimator for producing a single beam of x-rays to interact with the organ. First generation computed tomography scanners were able to measure the amount of x-rays passing through the organ successfully by using only two detectors located on the opposite sides of the body organ. Time taken for imaging and their reconstruction was major drawback of first generation computed tomography scanners [29].

2.2.2 Second generation: Second generation of computed tomography scanners was introduced with a narrow fan x-rays beam with an angle of 10° approximately in the form of a linear array of 30 detectors. The largest advantage associated with second generation scanners was the substantial decrease in time in comparison to first generation. Unlike pencil beam, narrow fan beams contribute to scattering and hence detectors were exposed to more scattered beams resulting in decreased resolution of images. Similar to first generation CT scanners, second generation CT scanners also require the rotation and translation of x-ray beams and hence capable for imaging of head only [30].

2.2.3 Third generation: Further to second generation usage of wide x-rays fan beam of angular range between 40° to 60° reduced the consumption of imaging time to 5-20 seconds in third generation of computed tomography scanners. Detectors were in the form of an array of 400-1000

detecting elements. A wide x-ray fan beam and detectors were joined so that they can rotate synchronously to produce faster imaging. Due to presence of a large number of detectors and uncalibrated detectors third generation CT scanners produce a ring artifact [31-32].

2.2.4 Fourth generation: Fourth generation of computed tomography scanners had around 5000 stationary detectors with perfect synchronization and calibration, arranged in the ring of 360° . Images from these scanners were reconstructed by x-rays fan beams obtained from the rotating x-rays tube. Due to this feature of the set-up, fourth generation CT scanners were specified as rotate-stationary geometry [33-35].

2.2.5 Fifth generation: Specially for cardiac tomography fifth generation of computed tomography scanners also known as cine-CT scanners or electron beam scanners were designed with no moving parts and referred to as stationary/stationary geometry. In fifth generation CT scanners the patient lies in the target of a large x-rays tube and electron beam after deflection produces x-rays which were detected by detectors. These scanners were able to capture unique contractions and relaxations of heart with a very high speed of imaging acquisition of the order of 50 msec [36].

2.2.6 Sixth generation: To overcome the gantry related difficulties of previous generation in 1990s sixth generation of computed tomography scanners with helical geometry introducing the slip ring technology for imaging were designed. This generation was the combination of the principles of third and fourth generation. The acquisition time for this generation was very small (i.e. the entire abdomen scanning took around 30 seconds). The data provided by these CT scanners in helical form was the measure drawback of this generation [37].

2.2.7 Seventh generation: Seventh generation of computed tomography scanners is the most recent with cone shaped x-rays beam and multiple detectors. The linear detector array of the previous generation is modified to flat panel detector or to multiple detectors array [38]. Imaging speed and their reconstruction are very outstanding with the combination of cone shaped x-rays beam and paneled detectors, which can acquire very large number of slices in very short time period.



Figure1. Siemens-Somatom Sensation open CTScanner at Dr. Ram Manohar Lohia Institute of Medical Sciences Lucknow, Uttar Pradesh, India

2.2 Advanced Techniques used in External Beam Radiation Therapy

Radiation delivering technologies and dose escalations for target volume in external beam radiation therapy had improved with time. Megavoltage external beam radiation therapy is usually delivered by Cobalt units (isotope Co^{60} , atomic number 27, mass number 60, mean energy 1.25 MeV, half life 5.26 years and γ -ray constant 1.33 Rontgen/hour-currie at 1 meter distance) in regular practices as the main stay in a radiation source [39]. Selection of beam energy for available technology depending on the depth of tumor has become a standard practice to deliver tumoricidal dose. High energy clinical linear accelerators with On-Board-Imaging (OBI) and computer controlled multileaf collimating (MLC) systems (as shown in figure 2) has escorted prototype changes in radiation therapy practices. It makes possible to deliver the

escalated dose to targeted volume and minimized dose within tolerance limits to normal tissues. These radiation techniques deliver highly conformal and homogeneous radiation dose to target with positional accuracy less than 1 mm.

In general a linear accelerator can provide 2-3 photon energies and 4-7 electron energies. The dual energy Clinical Linear accelerators offer an option to select photon energy depending on the depth of tumor. The superficial tumors are treated by low energy photon beam with small penetration depth and the deep seated tumors are treated by high energy photon beam with large penetration depth [40-42]. The electron beam has very small penetration power and found to be very useful for treating the superficial tumor upto 6 cm depth. Most useful range of energy for electron beams is 6-15 MeV.



Figure 2. Clinical linear asclerator “Elekta Synergy” with Multileaf collimator at Dr. Ram Manohar Lohia Institute of Medical Sciences, Lucknow, Uttar Pradesh, India

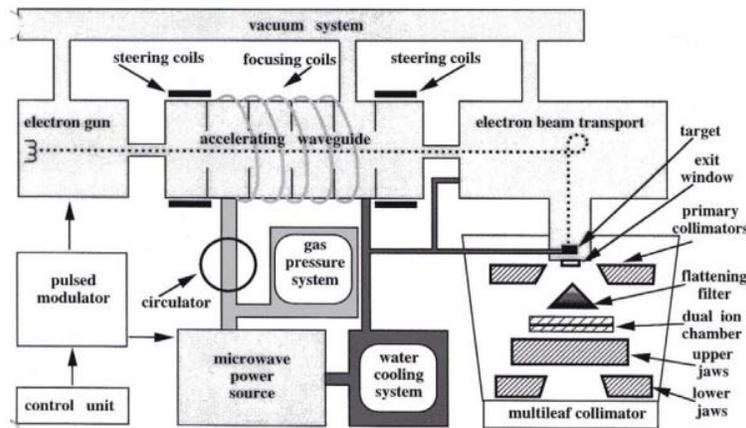


Figure 3. Schematic diagram of Clinical Linear Accelerator with multileaf collimator.

However, in some cases photon beams are used in combination of electron beam to boost superficial nodes after the completion of photon beam treatment. The electron beams are frequently used for irradiation of chest wall carcinoma of breast

and to boost the nodes in head and neck tumors. Table 1 below is an outlook to provide information about the x-rays and electron energies available from Clinical Linac in present time [42].

Table 1. Photon and Electron energies received from a Clinical Linear Accelerator: An experimental data showing maximum depth dose for photon beam and 90% 80 % dose depth for electron beam.

Sl.No.	Photon		Electron		
	Energy (MV)	Max. Dose Depth (cm)	Energy(Me V)	90% Dose Depth (cm)	80% Dose Depth (cm)
1.	4	1.0	4	1.1	1.3
2.	6	1.6	6	1.5	2.0
3.	10	2.5	9	2.2	3.0

4.	15	2.8	12	3.0	4.0
5.	18	3.5	15	3.7	5.0
6.	24	4.0	18	4.5	6.0
7.	--	-----	21	5.2	7.0

2.3 Treatment Planning System (TPS) in Advanced External Beam Radiation Therapy

Treatment planning system (TPS) being the backbone of radiation therapy system is a key to improve the outcomes of radiation therapy. TPS provides various treatment options in very efficient manner for radiation therapy. Its outstanding features not only reduce pre treatment planning time but also yield alternatives like self image fusion and fast organ delineation [43-45]. Various advanced treatment techniques to define the best treatment plan are contributed by TPS systems. TPS reinforce are wide range of treatment techniques including two dimensional (2D), three dimensional (3D), MLC based IMRT, SRS, SRT etc. Its advanced tools ease the contouring delineation & field setup and its high speed calculation engine minimize the typical planning time. The high resolution and less delivery time of TPS reduce the delivery time of advanced treatment modalities to 10-15 minutes on a Clinac with advanced TPS. The option for plan verification and quality assurance provided by TPS systems help Physicists to save time and increase accuracy of the system [46].

TPS systems came into existence in 1980s when one dimensional planning was done manually. 2D-CT based TPS was developed during 1980-1990s with the involvement of computers. After 1990s processes of dose calculations inside inhomogeneous human tissues were enhanced with development of different algorithms like pencil-beam, convolution, Clarkson, FFT Convolution, Multi Grid Superposition, Electron Monte Carlo and Fast Superposition etc. 3D dose calculations came into existence by 1995s and 4D dose calculations with increased outcomes of radiation therapy and real time motion of patient during the treatment were developed upto 2000 [47]. Data sets of CT imaging of the target are directly loaded to the computer system for processing and then TPS system creates a typical complex treatment plan for each beam line and directs the system to deliver the therapy. Computer software calculates the desired dose distribution for the various inhomogeneities of the patient body like bones, lungs, muscles etc.

Involvement of TPS is very fruitful in maximizing the dose to tumor site as well as escaping the critical structures from radiation effects to avoid their damage complications. TPS includes all the beam arrangement and automatic beam modification devices to modify the beam around critical structures. Automated complex programming of TPS for multi-leaf-collimators is capable to block the critical structures during the treatment delivery [48]. Beam modification facility provided by TPS can modify the beam in case shrinkage of tumor during the treatment time. XiO, Eclipse, Pinnacle, Oncentra, Prowess etc. are various TPS systems used in present time. TPS also gives a choice to choose appropriate algorithm for treatment depending on requirement of case [49].

III. CONCLUSION

The present study gives an outlook towards the basic concepts involved related to radiation therapy. This study also

gives a brief idea of the development of the various techniques of radiation therapy involve wide range of energies from x-ray, γ -ray and charged particles. By using this study it is concluded that electron beam external radiation therapy is more suitable for superficial tumors like nasal nodes, head and neck cancers and breast carcinomas. It is also beneficial in providing the radiation boost to the residual cancers after surgery. Since the energy of the beam drop off rapidly after the desired depth, so that the sensitive body parts can be escaped from the radiation effects.

ACKNOWLEDGEMENT

The author acknowledges that this article has prepared under the supervision of Professor Asita Kulshreshtha, head of Amity school of applied sciences, Amity University Uttar Pradesh, Lucknow and Dr. Anoop Kumar Srivastava, Associate Professor, Department of radiation oncology, Dr. Ram Manohar Lohia Institute of Medical Sciences, Lucknow, Uttar Pradesh.

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AUTHORS

First Author – Sant Pal Singh, Amity School of Applied Sciences, Amity University Uttar Pradesh, Lucknow, santpal.ydic.oel@gmail.com

Second Author – Asita Kulshreshtha, Amity School of Applied Sciences, Amity University Uttar Pradesh, Lucknow, akulshreshtha@amity.edu

Third Author – Anoop Kumar Srivastava, Dept. of Radiation Oncology, Dr. RML Institute of Medical Sciences, Lucknow, dranooprmlims@gmail.com

Fourth Author – Sumit Kumar Srivastava, Amity School of Applied Sciences, Amity University Uttar Pradesh, Lucknow, sumit.astro.physics@gmail.com